

COLLECTION WELL FOR BODY FLUID TESTER

TECHNICAL FIELD

This invention pertains to testing a body fluid for an analyte. For example, the present invention is applicable for testing glucose in a body fluid such as blood or interstitial fluid.

BACKGROUND

Numerous patents teach various ways for collecting a sample of body fluid and testing such fluid for an analyte such as glucose. For example, United States Patents 5,823,973 and 5,820,570 describe methods and apparatus for obtaining, in one embodiment, interstitial fluid, which is tested for glucose through IR absorption. These patents also describe use of the disclosed inventions in colormetric and electro-chemical testing of glucose. U.S. Pat. No. 5,453,360 teaches a test strip for colormetric testing for glucose. Blood is placed on a test strip containing various chemical components including a dye. The degree of color change of the test strip indicates the amount of glucose. United States Patents 5,508,171 and 5,628,890 teach electro-chemical testing. Blood is placed on a test strip containing electrodes. Reaction of glucose on the electrodes generates a current indicating the amount of glucose present in the blood.

Present development efforts are directed to testing very small volumes of body fluid (e.g. about 0.5 microliter). The use of such small volumes of fluid permits less painful collection of a fluid samples. However, small fluid volumes present additional challenges for analyte testing. For example, testing for analytes typically requires a fluid sample in excess of a predetermined minimum volume. By way of non-limiting representative example, a test may require a minimum sample size of 5 microliter to yield reliable test results.

Furthermore, sample collection systems may receive a flow of body fluid over an extended time (e.g., 10 seconds or more) before a minimum sample volume is collected.

As a result, body fluid may be deposited on test components (e.g., electrodes or colormetric test strips) before a full sample is collected. Such premature deposit may initiate chemical reactions on a test strip thereby consuming reagents before a reliable test can be initiated. Further, such test components may be coupled to logic circuits for calculating an analyte's concentration based on readings from the test strip. A premature deposit of an inadequate volume of fluid sample may falsely inform logic circuits that testing has initiated when, in fact, an adequate sample volume has yet to be collected.

Recognizing the problems of premature test initiation, the prior art has developed techniques for delaying test initiation until an adequate volume of sample is collected. For example, logic circuits may have a built-in time delay which assumes a fixed period of time to collect an adequate volume of sample. Of course, such systems suffer from the fact there is no certainty that an adequate volume is collected during such time delay. Alternatively, to be conservative, such time delays may frequently be unnecessarily long. Additionally, United States Patent 5,049,487 teaches reading a reflectance of a side of a membrane. A fluid sample is placed on the opposite side. When the sample is absorbed through the membrane, the change in reflectance is noted indicating testing may commence. However, such a system suffers from chemical agents on the membrane being in contact with a sample prior to initiating testing.

Therefore, there is a need for a method and apparatus for collecting a sample of body fluid to obtain an adequate volume of such fluid.

SUMMARY

According to a preferred embodiment of the present invention, a method and apparatus are disclosed for collecting a body fluid for testing for an analyte contained within the body fluid. The apparatus includes a reservoir for receiving and collecting a flow of body fluid from a discharge end of a conduit. A capillary test space is in fluid flow communication with the reservoir. The capillary test space is positioned to be in contact with the fluid in the reservoir after the fluid has accumulated to a predetermined transfer volume of fluid. The capillary test space is sized to wick the fluid from the reservoir when the fluid contacts the entrance end. With the present invention, fluid is

collected within the reservoir at a rate of flow limited by the conduit. When the reservoir is full, the collected fluid rapidly wicks into the capillary test space. The capillary test space may contain test components for testing for the analyte.

BRIEF DESCRIPTION OF THE DRAWINGS

Fig. 1 is a perspective view of a sample collection apparatus with an electro-chemical test strip shown removed;

Fig. 2 is an enlarged segmented view of the area of circle 2 in Fig. 1;

Fig. 3 is a side-sectional view of the apparatus of Fig. 1 showing the test strip in place;

Fig. 4 is an enlarged segmented view of the area of circle 4 in Fig. 3;

Fig. 5 is a segmented top-plan view of a reservoir of the apparatus of Fig. 1;

Fig. 6 is a view taken along line 6-6 in Fig. 3 and showing a bolus of body fluid residing in a capillary test space;

Fig. 7 is a top plan view of a first alternative embodiment of the present invention;

Fig. 8 is a view taken along line 8 – 8 of Fig. 7;

Fig. 9 is a view similar to Fig. 8 showing a second alternative embodiment of the present invention;

Fig. 10 is a view similar to those of Figs. 8 and 9 showing a third alternative embodiment of the present invention;

Fig. 11 is a top plan view of the embodiment of Fig. 10 with a test strip removed; and

Fig. 12 is a view similar to Fig. 11 showing a fourth alternative embodiment of the present invention

DETAILED DESCRIPTION

With reference to the various drawing figures in which identical elements are numbered identically throughout, a description of a preferred embodiment will now be provided. Throughout this description, the present invention will be described with reference to collecting a sample of interstitial fluid for glucose testing using a narrow

needle that penetrates into, but not through, the dermis as more fully described in commonly assigned United States Patents 5,823,973 and 5,820,570, the disclosures for both of which are hereby incorporated herein by reference. While such a use is a preferred embodiment, the present invention is applicable to other fluid collection systems (e.g., blood collection) as well as testing for other fluid analytes. Further, the present invention is described with reference to using electro-chemical testing of a collected sample. The teachings of the present invention are equally applicable to other testing methods such as colormetric testing and IR absorption testing.

Referring now to Figures 1-6, a collection apparatus 10 includes a main body 12 and a test strip 14. The main body has a handle 16 and a needle-containing ferrule 18. The ferrule 18 holds a hollow needle 20 extending from a penetration end 22 to a discharge end 24. The penetration end 22 protrudes from a radially spaced ring end 26 of the ferrule 18.

In a preferred embodiment, the penetration end 22 is axially spaced from ring end 26 by a distance sufficient for the needle 20 to penetrate into but not through a patient's dermis to collect a sample of substantially blood-free interstitial fluid as taught in United States Patent 5,820,570. In such an embodiment, the outer diameter of the needle is about .013 inch (about 0.33 mm). This sizing of the needle permits substantially pain-free penetration of the needle to collect a body fluid. This description illustrates a preferred embodiment. Needle 20 may be sized to collect any body fluid such as blood or interstitial fluid. Further, the present invention is disclosed where the skin penetration member (i.e., the needle 20) also serves as a conduit for supplying fluid to a reservoir 30 as will be described. The present invention is also applicable to any conduit for transporting a body fluid (e.g., a capillary tube as described in International Application PCT/US97/08400 published November 20, 1997 as International Publication No. WO 97/42883).

The test strip 14 contains exposed test components on an inner surface 14a. The test components are shown in the form of electrodes 32 for testing a body fluid for an analyte such as glucose through electro-chemical testing. As previously described, the

test components could be components for alternate testing techniques such as colormetric or IR absorption testing.

Not shown is a housing for holding the apparatus 10 during sample collection and testing. Housings for holding disposable body fluid samplers are shown in United States Patent 5,823,973. Such housings may contain electrical components for electrical connection to the test strip electrodes 32 to connect a signal from the electrodes 32 to logic circuits to compute and report on the analyte in response to signals from the electrodes 32 during testing.

The material of the main body 12 defines a cylindrical reservoir 30 having a cylindrical axis between a first end 34 and a second end 36. In the embodiment shown, the axis of the reservoir 30 is perpendicular to the axis of the needle 20. Such a relative alignment is not necessary for adequate function and any other alignment is acceptable.

The reservoir 30 has a volume at least as great as a desired test volume of body fluid to be tested. In a preferred embodiment, reservoir 30 has a volume of 0.7 microliters. As will become apparent, fluid is collected in the reservoir 30 and accumulates with a fluid level rising from the first end 34 toward the second end 36. Due to such small volumes and the geometry of reservoir 30, surface tension assures the fluid is retained in the reservoir 30 with the fluid level rising as described regardless of the orientation of the apparatus 10 (i.e., the operation of the apparatus 10 is gravity independent).

The discharge end 24 of the needle 20 is disposed within the reservoir 30 adjacent the first end 34. Accordingly, body fluid is transported from the penetration end 22, through needle 20 and discharged from the discharge end 24 into the reservoir 30 at the first end 34.

The material of the body 12 also defines an enlarged empty volume 38 positioned between the reservoir 30 and the ferrule 18 and surrounding the needle 20. The enlarged volume 38 is separated from the reservoir 30 by material of the main body pinching against the needle 20 as at locations 40. The enlarged volume 38 has a volume larger than the reservoir 30 and ensures that fluid within the reservoir 30 is retained within reservoir 30 as it accumulates. For example, in the absence of enlarged volume 38,

manufacturing tolerances may result in a narrow spacing between the material of main body 12 and needle 20. Such a narrow spacing could function as a capillary space communicating with reservoir 30 which would wick fluid out of reservoir 30. The enlarged volume 38 precludes such capillary wicking. Further, the material defining the volume 38 is preferably hydrophobic to minimize wicking. In the event precise manufacturing permits complete liquid-tight sealing around needle 20, the enlarged volume 38 could be eliminated.

The test strip 14 is secured to the main body (e.g., through adhesives) with the inner surface 14a facing the main body 12 and overlying the second end 36 of the reservoir 30. The main body 12 includes a groove 42 shaped complementary to the outer periphery of the test strip 14 to ensure accurate alignment of the test strip 14 with the main body 12. Adjacent its outer periphery, the inner surface 14a of the test strip 14 includes spacers 44 (shown best in Fig. 6). The spacers 44 insure uniform and close parallel spacing of the inner surface 14a from a test strip opposing surface 12a of the main body 12 for reasons that will become apparent. Alternatively, spacers could be formed on the body 12 thereby eliminating the need for spacers 44.

The test strip opposing surface 12a includes a step 46. With reference to Fig. 6, the construction described above results in formation of a capillary test space 48 defined between opposing surfaces of the test strip inner surface 14a and step 46.

As shown in Fig. 6, the spacers 44 are spaced from opposing surfaces of the step 46 thereby defining enlarged volumes 50 on opposite sides of the step 46. The enlarged volumes 50 perform a function similar to that of enlarged volume 38. Namely, if the spacers 44 were sized to abut step 46, small capillary spaces could form between the spacers 44 and step 46. Such capillary spaces could wick fluid from the fluid receiving volume 48. Again, if manufacturing could ensure a fluid-tight seal between spacers 44 and step 46, the volumes 50 could be eliminated.

Shown best in Figs. 4 and 6, the electrodes 32 are positioned opposing the step 46. Further, the spacing S (Fig. 4) between the step 46 and inner surface 14a is uniform and is selected to be sufficiently narrow for the capillary test space 48 to act as a capillary space to wick fluid from the reservoir 30. An entrance end 52 of the capillary test space 48 is

positioned at the second end 36 of the reservoir 30 (Fig. 4). The preferred spacing S is about .003 -- .005 inch (about .075 mm to .125 mm). The spacing S may be as large as .012 inch (about .300 mm) or larger depending on the surface tension and volume of the fluid being collected and the relative hydrophobic/hydrophilic characteristics of the main body 12 and test strip 14.

A hole 54 is formed through the body 12 and into the fluid receiving volume 48 on a side of the step 46 opposite the reservoir 30. The hole 54 permits air in the capillary test space 48 to be vented to atmosphere as fluid flows into the capillary test space 48 from the reservoir 30. Volumes 50 also provide venting.

An additional advantage of this embodiment is its ability to minimize the effects of sample concentration via evaporation. The total air volume contained within the enclosed sections substantially defined by volume 38, reservoir 30, the capillary test space 48, and adjoining volumes spaces, is sufficiently small so as to provide a very low capacity for evaporation of water from the aqueous sample being collected. In addition, the location of the vent and the overall geometry discourage convective passage of air through the aforementioned spaces, minimizing any convective acceleration of evaporation. When dealing with small volumes (e.g. less than 1 microliter), minimizing evaporative losses can be important to maintaining the integrity of the sample for quantitative analysis.

With the construction thus described, the apparatus 10 is used by urging the ring end 26 against a patient's skin. The penetration tip 22 penetrates the skin. The ring end 26 (being radially spaced from tip 22) acts to urge fluid into the needle 20. The fluid flows along the needle 20 and discharges into the first end 34 of the reservoir 30 through discharge end 24. In one possible embodiment, suction could be applied to advance the rate of flow of fluid through needle 20. Suction is not used in other embodiments.

Fluid accumulates in the reservoir 30 with a level of accumulated fluid growing from the first end 34 to the second end 36. When the fluid level reaches the second end 36, a desired volume of fluid to be tested has accumulated in the reservoir 30. At this

time, the fluid level contacts the entrance end 52 of the capillary test space 48. Since the capillary test space 48 is a narrow capillary space, the fluid is rapidly wicked out of the reservoir 30 and into the capillary test space 48 as a bolus delivery of fluid indicated by the bolus of fluid 56 in Fig. 6. So positioned, the fluid is in contact with the electrodes 32 and testing of the fluid may commence.

The present invention permits fluid contact with the electrodes 32 only after an adequate volume of fluid has been collected. By way of non-limiting representative example, it may take thirty seconds for fluid to fill the reservoir 30 and only one second for the accumulated fluid to be wicked into the capillary test space 48 from the reservoir 30. As a result, the present invention avoids a long period of time during which fluid is contacting the electrodes 32 and before testing may commence. Further, without the need for specialized electronics as used in the prior art, testing cannot commence until after an adequate volume of fluid has been accumulated. Therefore, when a signal is received from electrodes 32, it is known that an adequate volume of fluid is opposing the electrodes 32.

The retention of fluid in the reservoir 30 and wicking of fluid into the capillary test space 48 can be controlled and modified by varying the dimensions of the components as will be apparent to one of ordinary skill in the art having the benefit of the teachings of the present invention. Further, as will be apparent to such artisan, such retention and wicking may also be controlled and modified through material selection. For example, it is desirable that the main body 12 be formed of hydrophobic material and that the capillary test space 48 be more hydrophilic. For example, a hydrophilic surfactant may be applied to step 46 or test strip inner surface 14a (or both) to make the capillary test space 48 more hydrophilic than the reservoir 30.

It may be desirable to have one of electrodes 32 completely wetted with fluid from reservoir 30 before the other of the electrodes 30 is wetted. Figs. 7 – 12 illustrate several alternative embodiments for achieving such sequential wetting. In the embodiments, elements in common with those already described are numbered identically with the addition of letter suffices (i.e., "a", "b", "c" and "d"). Such elements are not separately described unless modified by the alternative embodiment.

In Figs. 7 and 8, it is desirable to completely wet electrode 32a before wetting electrode 32a'. The electrodes 32a, 32a' are positioned side-by-side on test strip 14a and equidistant from reservoir 30a. As shown in Fig. 8, the step 46 of the previously described embodiment is divided into two steps 46a, 46a' opposing respective ones of electrodes 32a, 32a'. A hydrophobic volume 50a' is positioned between the steps 46a, 46a'. The volume 50a' functions similarly to side volumes 50a (and 50 in the embodiment of Fig. 6) to act as a hydrophobic barrier to prevent fluid from flowing between the steps 46a, 46a'. The steps 46a, 46a' are spaced from test strip 14 by spaces Sa and Sa'. Since space Sa is smaller than space Sa', fluid first flows from reservoir 30a into space Sa before flowing from reservoir 30a into space Sa'.

In the embodiment of Fig. 9, fluid is inclined to first flow onto step 46b before onto step 46b'. However, in Fig. 9, the volume barrier 50a' of Fig. 8 has been replaced with a ramp surface 47b connecting steps 46b and 46b'. Therefore, fluid can flow from space Sb to space Sb' after space Sb has first filled with fluid.

In the embodiment of Figs. 10 and 11, the steps 46c, 46c' are positioned on opposite sides of the reservoir 30c. If spaces Sc and Sc' are equal, fluid flows simultaneously into the spaces Sc and Sc' but does not flow between the spaces Sc and Sc'. The spaces Sc and Sc' may be varied to change the rate of flow into the spaces Sc and Sc'.

The embodiment of Fig. 12 is similar to that of Fig. 9. Instead of the ramp 47b of Fig. 9 (which connects steps 46b and 46b' directly across a side-to-side path), the ramp 47d is U-shaped for fluid to flow from step 46d to step 46d' in a U-shaped path A on a side of the steps 46d, 46d' opposite the reservoir 30d.

From the foregoing detailed description, the present invention has been described in a preferred embodiment. Modifications and equivalents of such disclosure are intended to be included in the appended claims. For example, either or both of the reservoir 30 and capillary test space 48 need not be an empty volume but could be filled with an absorbent material.